FORM PTO-1390 (Modified) (REV 11-2000) U.S. DEPARTMENT OF COMMERCE PATENT AND TRADEMARK OFFICE 8830-20 TRANSMITTAL LETTER TO THE UNITED STATES U.S. APPLICATION NO. (IF KNOWN, SEE 37 CFR DESIGNATED/ELECTED OFFICE (DO/EO/US) CONCERNING A FILING UNDER 35 U.S.C. 371 INTERNATIONAL APPLICATION NO. INTERNATIONAL FILING DATE PRIORITY DATE CLAIMED September 7, 1999 PCT/GB00/03424 September 7, 2000 TITLE OF INVENTION CELL GROWTH SUBSTRATE APPLICANT(S) FOR DO/EO/US THOMAS GILCHRIST AND DAVID MICHAEL HEALY Applicant herewith submits to the United States Designated/Elected Office (DO/EO/US) the following items and other information: This is a FIRST submission of items concerning a filing under 35 U.S.C. 371. 2. This is a SECOND or SUBSEQUENT submission of items concerning a filing under 35 U.S.C. 371. This is an express request to begin national examination procedures (35 U.S.C. 371(f)). The submission must include itens (5), (6), 3. \boxtimes (9) and (24) indicated below. \boxtimes The US has been elected by the expiration of 19 months from the priority date (Article 31). 4. A copy of the International Application as filed (35 U.S.C. 371 (c) (2)) 5. X is attached hereto (required only if not communicated by the International Bureau). a. 🗌 b. 🖾 has been communicated by the International Bureau. is not required, as the application was filed in the United States Receiving Office (RO/US). c. [] An English language translation of the International Application as filed (35 U.S.C. 371(c)(2)). a. 🔲 is attached hereto. has been previously submitted under 35 U.S.C. 154(d)(4). Amendments to the claims of the International Application under PCT Article 19 (35 U.S.C. 371 (c)(3)) are attached hereto (required only if not communicated by the International Bureau). have been communicated by the International Bureau. b. have not been made; however, the time limit for making such amendments has NOT expired. c. 🖂 have not been made and will not be made. An English language translation of the amendments to the claims under PCT Article 19 (35 U.S.C. 371(c)(3)). 8. 9. \boxtimes An oath or declaration of the inventor(s) (35 U.S.C. 371 (c)(4)). An English language translation of the annexes to the International Preliminary Examination Report under PCT 10 Article 36 (35 U.S.C. 371 (c)(5)). 11. \boxtimes A copy of the International Preliminary Examination Report (PCT/IPEA/409). 12. \boxtimes A copy of the International Search Report (PCT/ISA/210). Items 13 to 20 below concern document(s) or information included: \boxtimes An Information Disclosure Statement under 37 CFR 1.97 and 1.98. \boxtimes An assignment document for recording. A separate cover sheet in compliance with 37 CFR 3.28 and 3.31 is included. 14 15 \boxtimes A FIRST preliminary amendment. 16. A SECOND or SUBSEQUENT preliminary amendment. 17. A substitute specification. A change of power of attorney and/or address letter. 18. A computer-readable form of the sequence listing in accordance with PCT Rule 13ter.2 and 35 U.S.C. 1.821 - 1.825. 19. A second copy of the published international application under 35 U.S.C. 154(d)(4). 20. A second copy of the English language translation of the international application under 35 U.S.C. 154(d)(4). 21 \boxtimes Certificate of Mailing by Express Mail 22. Other items or information: 23 U.S. Express Mail No. EL 931089991 US Courtesy Copy Of the Publication of PCT/GB00/03424

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PATENT

Attorney Docket No.: 8830-20

IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

In re:

Patent application of Thomas Gilchrist et al.

: Group Art Unit:

Serial No:

Not yet assigned

(International Application No: PCT/GB00/03424)

Filed:

Herewith

(International Application: Sept. 7, 2000)

: Examiner:

For:

CELL GROWTH SUBSTRATE

PRELIMINARY AMENDMENT

Commissioner for Patents Washington, D.C. 20231 Sir:

Kindly amend the above-identified application, without prejudice, in advance of calculating the filing fee. A mark-up of the amended claims is contained in Appendix A hereto.

In the Specification:

Insert the abstract submitted herewith on a separate page.

CERTIFICATE OF MAILING UNDER 37 C.F.R. 1.10

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Date of Deposit: February 22, 2002

I hereby certify that this correspondence, along with any paper referred to as being attached or enclosed, and/or fee, is being deposited with the United States Postal Service, "EXPRESS MAIL-POST OFFICE TO ADDRESSEE" service under 37 C.F.R. 1.10, on the date indicated above, and addressed to: Commissioner for Patents, Washington, D.C. 20231.

Signature of person mailing page:

Therese McKinley

Type or print name of person

In the Claims

Rewrite claims 3, 4, 5, 6, 8, 9, 10, 12, 14, 16 and 18 to read as follows:

- 3. (amended) The substrate of Claim 1, wherein said matrix has at least a portion of its surface coated with living cells.
- 4. (amended) The substrate of Claim 1, wherein the water-soluble glass is a phosphate glass.
- 5. (amended) The substrate of Claim 1, wherein said water-soluble glass comprises phosphorus pentoxide as glass former.
- 6. (amended) The substrate of Claim 1, wherein said glass comprises an oxide or a carbonate of an alkali metal, an alkaline earth metal or a transition metal as glass modifier.
- 8. (amended) The substrate of Claim 1, wherein said water-soluble glass contains a boron containing compound.
- 9. (amended) The substrate of Claim 1, wherein said glass has a dissolution rate ranging from substantially zero to 2.0 mg/cm²/hour at 38°C.
- 10. (amended) The substrate of Claim 1, wherein said glass enables a controlled release of additives in an aqueous medium.
- 12. (amended) The substrate of Claim 1, wherein said water-soluble glass matrix comprises water-soluble glass fibres.
- 14. (amended) The substrate of Claim 1, wherein said water-soluble glass matrix comprises finely comminuted glass particles.
- 16. (amended) The substrate of Claim 14, wherein said glass particles have an average diameter of from 15 microns to 6 mm.

18. (amended) A method to encourage growth of living tissue by providing the substrate of Claim 1.

Please cancel Claim 17.

Remarks

Claims 1 to 16 and 18 to 19 are pending in the application. The claims have been primarily amended to reduce dependencies and more closely conform to United States practice. The specification was not amended in the international phase.

Respectfully Submitted,
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APPENDIX A: Mark-up of amended claims

- 3. (amended) The substrate of Claim 1 [or 2], wherein said matrix has at least a portion of its surface coated with living cells.
- 4. (amended) The substrate of [any one of Claims] <u>Claim</u> 1 [to 3], wherein the water-soluble glass is a phosphate glass.
- 5. (amended) The substrate of [any one of Claims] <u>Claim</u> 1 [to 4], wherein said water-soluble glass comprises phosphorus pentoxide as glass former.
- 6. (amended) The substrate of [any one of Claims] <u>Claim 1</u> [to 5], wherein said glass comprises an oxide or a carbonate of an alkali metal, an alkaline earth metal or a transition metal as glass modifier.
- 8. (amended) The substrate of [any one of Claims] <u>Claim 1</u> [to 7], wherein said water-soluble glass contains a boron containing compound.
- 9. (amended) The substrate of [any one of Claims] <u>Claim 1</u> [to 8], wherein said glass has a dissolution rate ranging from substantially zero to 2.0 mg/cm²/hour at 38°C.
- 10. (amended) The substrate of [any one of Claims] <u>Claim 1</u> [to 9], wherein said glass enables a controlled release of additives in an aqueous medium.
- 12. (amended) The substrate of [any one of Claims] <u>Claim 1 [to 11]</u>, wherein said water-soluble glass matrix comprises water-soluble glass fibres.
- 14. (amended) The substrate of [any one of Claims] <u>Claim 1</u> [to 10], wherein said water-soluble glass matrix comprises finely comminuted glass particles.

- 16. (amended) The substrate of Claim 14 [or 15], wherein said glass particles have an average diameter of from 15 microns to 6 mm.
- 18. (amended) A method to encourage growth of living tissue by providing the substrate of [Claims] Claim 1[to 16].

CELL GROWTH SUBSTRATE

Abstract of the Disclosure

A cell culture growth substrate comprising a water soluble glass matrix adapted to sustain growth of living cells. Preferably the substrate comprises or is coated with living cells. The water-soluble glass is advantageously phosphate based and comprises glass fibres or finely comminuted particles. The invention also relates to the use of the growth substrate as an implant to replace or promote repair of damaged tissue in a patient and to a method to encourage growth of living tissue.

CELL GROWTH SUBSTRATE

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2	
3	The present invention provides a growth substrate for
4	cell culture. In particular, the present invention
5	provides a cell culture growth substrate for tissue
6	engineering.
7	
8	Tissue engineering is expected to transform
9	orthopaedics treatments, cancer therapy and the
10	treatment of chronic degenerative diseases. Tissue
11	engineering concerns the provision of a graft
12	comprising living cells or suitable substrate to
13	sustain the growth of such cells which integrate into
14	the patient providing expedited wound healing and
15	repair or an alternative drug delivery or gene therapy
16	delivery system. The tissue engineering graft may be
17	an autograft, allograft or xenograft. Autografts are
18	formed with the patient's own cells, cultured with a
19	suitable growth medium or substrate. Allografts rely
20	upon cells donated from an alternative same species
21	source (including cadaver or foetal sources) whilst
22	xenografts rely upon cells donated from other species.

Both allografts and xenografts may be treated to

- 2 minimise autoimmune rejection of the graft following
- 3 implantation.

4

- 5 There are numerous potential applications for tissue
- 6 engineered grafts, including reconstructive surgery,
- orthopaedics or dental applications, burn treatments
- 8 or ulcer treatments (including venous ulcers and
- 9 diabetic foot ulcers). A number of tissue engineered
- 10 grafts have been described in the literature (see
- 11 Dutton, "Tissue Engineering", Genetic Engineering
- 12 News, Vol 18, No 8, April 15, 1998).

- 14 Examples of such tissue engineered grafts include
- 15 APLIGRAF (Trade Mark) which is a bilayer graft
- 16 including both differentiated keratinocytes and a
- 17 layer of fibroblasts in a collagen matrix. APLIGRAF
- 18 has been used as a skin graft, particularly for burns,
- 19 diabetic foot ulcers, excisional surgery and venous
- 20 ulcers (Bender, "Healing of Difficult to Heal Wounds
- 21 Using a Bilayered Skin Construct", 11th Annual
- 22 Symposium on Critical Issues in Surgery-Wound Healing,
- 23 Science and Technology, 3-5 December 1998, St Thomas,
- 24 US Virgin Islands). Other bioengineering skin
- 25 equivalents include INTEGRA (Trade Mark), a xenograft
- of bovine collagen, glycosaminoglycans (GAG) and
- 27 silastic sheet; ALLODERM (Trade Mark), an allograft of
- 28 treated cadaver skin; and DERMOGRAFT (Trade Mark), an
- 29 allograft of neonatal fibroblasts on a polyglactin
- 30 scaffold. Tissue engineered grafts for bone include
- 31 RAINBOW (Trade Mark) of IsoTis BV which is a
- 32 biomimetic coating which allows a bone-like layer to
- 33 grow over metal prosthesis and serves as a scaffold

3

for bone growth, and also EMBARC (Trade Mark) which is

2 a resorbable bone repair material.

3

- 4 Despite the numerous tissue engineering grafts
- 5 currently being developed, there is still a demand for
- 6 further and improved products. We have now found that
- 7 water-soluble glass acts as a support or matrix for
- 8 cell growth and hence the glass has utility in tissue
- 9 engineering.

10

- 11 The present invention thus provides a cell culture
- 12 growth substrate comprising a water-soluble glass
- 13 matrix adapted to sustain the growth of living cells.
- 14 Preferably the substrate will comprise or have at
- 15 least a portion of the surface thereof coated with
- 16 living cells.

17

- 18 In one embodiment the cell culture growth substrate is
- 19 pre-seeded with living cells and hence the matrix
- 20 comprises or has at least a portion of its surface
- 21 coated with living cells.

22

- 23 In one embodiment, the cell culture growth substrate
- 24 will be useful as an implant or tissue graft, i.e. is
- 25 designed for implantation into a patient to replace or
- 26 promote repair of damaged tissues.

- 28 The water-soluble glass matrix will of course be
- 29 biocompatible. Generally, the biodegradation of the
- 30 water-soluble glass following implantation of the
- 31 graft into a patient will be pre-determined to be
- 32 compatible with the timescale required for regrowth of
- 33 the tissues concerned.

	4
1	
2	The glass present in the graft acts as a cell support
3	matrix and will function as such in vivo. Thus the
4	graft can be used directly in vivo to provide a
5	temporary biodegradable scaffold which will encourage
6	ingrowth of surrounding tissues. In other embodiments
7	pre-seeding of the graft with a pre-selected cell
8	type, and optionally growth of that cell type, prior
9	to implantation may be desirable.
10	
11	In an alternative embodiment, the cell culture growth
12	substrate is intended for non-clinical purposes, for
13	example in bio-reactor and fermentation technologies
14	for the production of drugs and other biologically
15	derived chemicals. Organisms usually grow with
16	increased confluence on surfaces, and enzyme reactions
17	(and many other biochemical reactions) are generally
18	most efficient when the enzyme is bound to a reaction
19	surface. Beads, sinters and fibres can be used to
20	provide the required mechanical support, with large
21	(productive) surface areas and additional features
22	such as controlled inorganic micro-nutrient supply,
23	contamination control, pH buffering and a
24	biocompatible carrier which will allow the subsequent
25	transfer or filtration of cells, enzymes or other
26	components bound to its surface on completion of the
27	reaction stage.
28	
29	Conveniently the water-soluble glass matrix may be in
30	the form of water-soluble glass fibres and reference
31	is made to our WO-A-98/54104 which describes the
32	production of suitable glass fibres. Whilst the glass
33	fibres can be used in the form of individual strands,

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5

- 1 woven (e.g. a 1 x 1 basket weave) or non-woven mats
- 2 may also be produced from the fibres and used as the
- 3 matrix. The individual fibres of a non-woven mat may
- 4 be gently sintered together to obtain coherence of the
- 5 strands. Alternatively, the fibres may be used as
- 6 glass wool and this form of matrix is especially
- 7 suitable where the graft requires a 3D shape.

8

- 9 Alternatively, the water-soluble glass matrix may be
- 10 produced from finely comminuted glass particles. For
- 11 example, the particles may have an average diameter of
- 12 from 15 µm to 6 mm, preferably from 50µm to 6 mm.
- Optionally, the glass particles may be sintered
- 14 together to form a porous structure into or onto which
- 15 cells may be seeded and in this embodiment the glass
- 16 particles will have a preferred diameter of from 53 μm
- 17 to 2 mm, preferably 400 µm to 2 mm. Again, a three-
- 18 dimensionally shaped graft may be produced (if
- 19 necessary individually tailored to be compatible with
- 20 the wound site of the patient) from the sinter.
- 21 Alternatively, particles following a Fuller curve
- 22 packing distribution and having a range of diameters
- 23 of 0.3 mm to 5.6 mm may be used.

24

- 25 In a further embodiment the glass may simply be in the
- 26 form of a glass sheet, which may be substantially
- 27 planar or may be contoured to a required shape.
- 28 Etched, ground or patterned glass sheet may be used in
- 29 addition to plain surfaced glass.
- 30 The water-soluble glass preferably includes
- 31 phosphorous pentoxide (P_2O_5) as the glass former.

- 1 Generally the mole percentage of phosphorous pentoxide
- 2 in the glass composition is less than 85%, preferably
- 3 less than 60% and especially between 30-60%.

4

- 5 One or more oxides or carbonates of alkali, alkaline
- 6 earth and transition metals are preferably used as
- 7 glass modifiers.

8

- 9 Generally, the mole percentage of these oxides or
- 10 carbonates of alkali, alkaline earth and transition
- 11 metals is less than 60%, preferably between 40-60%.

12

- Boron containing compounds (e.g. B₂O₃) are preferably
- 14 used as glass additives.

15

- 16 Generally, the mole percentage of boron containing
- 17 compounds is less than 15% or less, preferably less
- 18 than 5%.

19

- Other compounds may also be added to the glass to
- 21 modify its properties, for example SiO₂, Al₂O₃, SO₃,
- 22 sulphate ions (SO₄²⁻) or transition metal compounds
- 23 (e.g. first row transition metal compounds).

- 25 Typically the soluble glasses used in this invention
- 26 comprise phosphorus pentoxide (P₂O₅) as the principal
- 27 glass-former, together with any one or more
- 28 glass-modifying non-toxic materials such as sodium
- oxide (Na₂O), potassium oxide (K₂O), magnesium oxide
- 30 (MgO), zinc oxide (ZnO) and calcium oxide (CaO). The
- 31 rate at which the glass dissolves in fluids is
- 32 determined by the glass composition, generally by the
- 33 ratio of glass-modifier to glass-former and by the

7

1 relative proportions of the glass-modifiers in the

2 glass. By suitable adjustment of the glass

3 composition, the dissolution rates in water at 38°C

4 ranging from substantially zero (i.e. just above zero)

5 to 25mg/cm²/hour or more can be designed. However, the

6 most desirable dissolution rate R of the glass is

7 between 0.001 and 2.0mg/cm²/hour.

8

9 The water-soluble glass is preferably a phosphate 10 glass, and preferably comprises a source of metal ions 11 or boron which confer either antimicrobial protection

or boron which confer either antimicrobial protection or enhanced cell growth, or both, or which are useful

trace elements. Examples include silver, copper,

14 magnesium, zinc, iron, cobalt, molybdenum, chromium,

manganese, cerium, selenium, and these metal ions can

16 be included singly or in any combination with each

other. Where silver ions are of interest, these may

18 advantageously be introduced during manufacture as

19 silver orthophosphate (Ag_3PO_4) . The glass preferably

20 enables controlled release of metal ions or boron and

21 other constituents in the glass and the content of

22 these additives can vary in accordance with conditions

of use and desired rates of release, the content of

24 silver generally being up to 5 mole %. While we are

25 following convention in describing the composition of

26 the glass in terms of the mole % of oxides, of halides

27 and of sulphate ions, this is not intended to imply

28 that such chemical species are present in the glass

nor that they are used for the batch for the

30 preparation of the glass.

The optimum rate of release of metal ions into an 1 aqueous environment may be selected by circumstances 2 and particularly by the specific function of the 3 The invention provides a means 4 released metal ions. 5 of delivering metal ions or boron to an aqueous medium 6 at a rate which will maintain a concentration of metal 7 ions or boron in said aqueous medium of not less than 0.01 parts per million and not greater than 10 parts 8 9 per million. In some cases, the required rate of release may be such that all of the metal added to the 10 system is released in a short period of hours or days 11 and in other applications it may be that the total 12 metal be released slowly at a substantially uniform 13 rate over a period extending to months or even years. 14 15 In particular cases there may be additional 16 requirements, for example it may be desirable that no 17 residue remains after the source of the metal ions is exhausted or, in other cases, where the metal is made 18 available it will be desirable that any materials, 19 other than the metal ions itself, which are 20 simultaneously released should be physiologically 21 In yet other cases, it may be necessary to 22 harmless. ensure that the pH of the resulting solution does not 23 fall outside defined limits. 24 25 26 Generally, the mole percentage of these additives in the glass is less than 25%, preferably less than 10%. 27 28 29 The cells may be any suitable cells required for 30 grafts. Particular mention may be made of 31 keratinocytes, fibroblasts, chrondrocytes and the like 32 as preferred cell types. Mention may also be made of

33 stem cells (mesenchymal, haematopoetic, and

9

- embryonic), Schwaan cells, keratinocytes (epithelial
- 2 cells), chondrocytes, osteoblasts, endothelial cells
- 3 and other fibroblasts, cardiac cells (and other
- 4 myoblasts), pancreatic β cells and periodontal tissues
- 5 e.g. Dentine, but the invention is not limited to
- 6 these cell types alone.

7

- 8 Embodiments of the invention will be described with
- 9 reference to the following non-limiting examples and
- 10 Figs. in which:

11

12 Fig. 1

13

- 14 Chondrocytes forming a monolayer on a glass fibre
- 15 (Example 1) as viewed by laser scanning confocal
- 16 microscope.

17

18 Fig. 2

19

- 20 Fluorescent microscopy of HUE cells on MATT01 glass
- 21 fibres (see Example 2).

22

23 Fig. 3

24

- 25 Fluorescent microscopy of HUE cells on MATT04 glass
- 26 fibres (see Example 2).

27

28 Fig. 4

29

- 30 SEM picture of L929 cells on glass surface at x30
- 31 magnification (see Example 3).

Fig. 5 SEM picture of L929 cells on glass surface at x170 magnification (see Example 3). Fig. 6 SEM picture of L929 cells on glass surface at x215 magnification (see Example 3). Fig. 7 SEM picture of L929 cells on glass surface at x610 magnification (see Example 3). Fig. 8 Bar chart showing cell activity vs. concentration for Ag/Mg in a PBS Extraction Vehicle (see Example 4). Fig. 9 Bar chart showing cell activity vs. concentration for Ag/Ni in a PBS Extraction Vehicle (see Example 4). Fig. 10 Bar chart showing cell activity vs. concentration for Ag/Zn in an MEM Extraction Vehicle (see Example 4).

	11
1	Fig. 11
2	
3	Bar chart showing cell activity vs. concentration for
4	Ag/B in a PBS Extraction Vehicle (see Example 4).
5	
6 7	<u>Fig. 12a</u>
8	Bar chart showing cell activity vs. concentration for
9	Mg/Cu in a PBS Extraction Vehicle (see Example 4).
10	
11	Fig. 12b
12	
13	Bar chart showing cell activity vs. concentration for
14	Mg/Cu in an MEM Extraction Vehicle (see Example 4).
15	
16	Fig. 13
17	
18	Bar chart showing cell activity vs. concentration for
19	Mg/Ni in a PBS Extraction Vehicle (see Example 4).
20	
21	Fig. 14a
22	
23	Bar chart showing cell activity vs. concentration for
24	Mg/B in a PBS Extraction Vehicle (see Example 4).
25	
26	Fig. 14b
27	
28	Bar chart showing cell activity vs. concentration for
29	Mg/B in a MEM Extraction Vehicle (see Example 4).
30	
31	
32	
33	

1	<u>F1G. 15a</u>
2	
3	Bar chart showing cell activity vs. concentration for
4	Ni/Cu in a PBS Extraction Vehicle (see Example 4).
5	
6	Fig. 15b
7	
8	Bar chart showing cell activity vs. concentration for
9	Ni/Cu in a MEM Extraction Vehicle (see Example 4).
LO	
Ll	Fig. 16
12	
13	Bar chart showing cell activity vs. concentration for
14	Ni/Zn in a PBS Extraction Vehicle (see Example 4).
15	
16	Fig. 17a
17	
18	Bar chart showing cell activity vs. concentration for
19	Ni/B in a PBS Extraction Vehicle (see Example 4).
20	
21	Fig. 17b
22	
23	Bar chart showing cell activity vs. concentration for
24	Ni/B in a MEM Extraction Vehicle.
25	
26	<u>Fig. 18</u>
27	
28	Bar chart showing cell activity vs. concentration for
29	Cu/Zn in a MEM Extraction Vehicle.
30	
31	
32	
22	

	13
1	Fig. 19
2	
3	Bar chart showing cell activity vs. concentration for
4	Cu/B in a MEM Extraction Vehicle.
5	
6	<u>Fig. 20</u>
7	
8	Bar chart showing cell activity vs. concentration for
9	Zn/B in a PBS Extraction Vehicle.
10	
11	Example 1
12	
13	Introduction
14	
15	Controlled Release Glass (CRG) is a phosphate-based
16	material which degrades at a predeterminable rate. The
17	potential for using CRG as a cartilage engineering
18	matrix has been assessed using isolated equine
19	chondrocytes with in-vitro techniques. The glass was
20	provided in fibrous form in three different
21	compositions. The three CRG compositions provided have
22 23	shown potential as a tissue engineering substrate.
24	Materials and Method
25	Materials and Method
26	A total of 200,000 chondrocytes isolated from horse
27	articular cartilage were added to each 2 cm well in a
28	24 well plate. Every well contained 0.02 grams of
29	glass fibre sample. Four different fibres F1 to F4
30	(diameters 20-30 μm) were analysed: F1 - containing
31	Fe ₂ O ₃ and NaF, F2 - containing Ce ₂ O ₃ and Se. The
3 L	$re_{2}O_{3}$ and Nar, r_{2} - containing $Ce_{2}O_{3}$ and Se_{-} The

32 composition of glasses used to form F1 to F4 are set

14

- 1 out below in Table 1. The culture medium (containing
- 2 10% FCS) was changed daily. At time periods of 3 days,
- 3 1 week and 2 weeks, the samples were stained using
- 4 rhodamine phalloidin and oregan green for the viewing
- 5 of actin and tubulin using a laser scanning confocal
- 6 microscope. At the same time periods, the cell
- 7 supernatant was removed and stored at -80°C until
- 8 analysis on cell viability and type II collagen
- 9 production could be performed. Production of type II
- 10 collagen was analysed by using RT-PCR analysis on the
- 11 cDNA from the chondrocyte population in contact with
- 12 the glass fibres. The total RNA was prepared from the
- 13 cell population by the addition of 1 ml of TRIzol
- 14 (SIGMA) to the cell population for 5 minutes. After
- 15 this time, the TRIzol was retrieved and stored at -80°C
- 16 until RT-PCR analysis could be carried out. The RT-PCR
- 17 analysis was performed by tagging with primers for
- 18 collagen type II and with gapDH for cell viability.

19

- 20 Zymography was also performed at time periods of 4
- 21 days, 1 week and 2 weeks for detection of matrix
- 22 metalloproteinases (MMP's) produced by the
- 23 chondrocytes.

Table 1

BATCH RECORD SELECTION

			15		
Form		F,C + R	F,C + R	F,R + C	₽. +
Solution Rates	Annealed Non-Annealed @ 37.5°C @ 37.5°C (mg.cm ⁻² .hr ⁻¹)	N/A	N/A	N/A	0.9614
Solutio	TOTAL Annealed @ 37.5°C (mg.cm ⁻² .hr ⁻¹)	N/A	N/A	N/A	0.331
	TOTAL	100 N/A	A/N 9.66	100	100
	လ စ			2.27	
	Ce ₂ O ₃		2.01	1.96	
	N P P	1.1		0.4	
	Fe ₂ O ₃	1.76	0.95	0.93	
noles	MnO Fe ₂ O ₃ NaF Ce ₂ O ₃ Se	5.75 1.5 1.76 1.1	5.82 1.52 0.95	5.68 1.49 0.93 0.4 1.96 2.27 100 N/A	
Formulation as mole%	K20 B203	5.75	5.82	5.68	5
rmulat	K ₂ 0				10
E	Mgo				4
	Ag ₂ 0 P ₂ 0 ₅	46.78	46.1	45.05	46
	Ag ₂ 0				m
	CaO	17.26	17.42	17.03	
	Na20 CaO	25.85	25.78	25.19 17.03	32
epo2		FI	F.2		

F=fibres; C=cullet; R=rods

16

Results and Conclusions

1

- 3 Chondrocytes adhered to all three types of fibre
- 4 sample. At the 3 day time period, the cells appeared
- 5 to be rounded. At 1 week and 2 weeks, confocal
- 6 microscopy indicated cell proliferation between all
- 7 time periods. At 1 week and 2 weeks, the cells were
- 8 elongated and formed a monolayer along the fibre length
- 9 as can be seen in Fig. 1.

10

- 11 The RT-PCR analysis showed that fibres F2 and F3 were
- 12 producing collagen type II up to and including the two
- 13 week time period indicating that the cells retained
- 14 their chondrocytic phenotype.

15

- 16 The zymography performed on F2 and F3 showed that the
- 17 cells in contact with these fibres produced MMP2 at all
- 18 three time periods, but in a greater quantity at 2
- 19 weeks than 1 week, and at 1 week than 4 days. This
- 20 increase of MMP2 production is expected, as the cells
- 21 were seen to have increased in number at these time
- 22 periods from the confocal microscope analysis.

- 24 In conclusion, all three fibres types showed cell
- 25 adherence and the chondrocytes adhered to F2 and F3
- 26 appear to retain the ability to produce type II
- 27 collagen.

17 1 Example 2 2 3 Biological Evaluation of Non-woven Mat Fibres 1. Objective 5 6 Using in-vitro techniques determine: 7 The cytotoxicity of a series of five nona. 8 woven mat CRG fibres. 9 The potential of the fibres as a cell 10 b. substrate matrix. 11 12 2. Scope 13 14 15 The test procedures apply to all fibre samples. 16 17 3. Equipment and Materials 18 19 3.1 Equipment 3.1.1 Laminar air flow hood 20 3.1.2 Incubator maintained at 37°C/5% carbon dioxide 21 22 3.1.3 Refrigerator at 4°C 3.1.4 Freezer at -18°C 23 3.1.5 Vacuum source 24 3.1.6 Phase contrast microscope 25 26 3.2 Materials 27 28 3.2.1 Sterile plastic-ware pipettes 29 3.2.2 Sterile glass pipettes 3.2.3 24 well Sterile dishes 30

3.2.4 Surgical grade forceps

3.2.5 Surgical grade scissors

31

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		18
1	3.2.6	Sterile Universal containers
2	3.2.7	L929 cell culture line (ATCC NCTC Clone 929)
3	3.2.8	Human Umbilical endothelial cells (primary
4		cell source, Liverpool Women's Hospital)
5	3.2.9	TCPS negative control
6	3.2.10	CRG fibres:
7		D021298F1 (MATT01)
8		D301198F1 (MATT02)
9		D100299F1 (MATT03)
10		D161298F2 (MATT04)
11		D171298F2 (MATT05)
12		All CRG fibres were supplied non-sterile in
13		quantities 8g-38g. The compositions of CRG
14		fibres used (MATT01 to 05) are set out below
15		in Table 2.

Table 2

BATCH RECORD SELECTION

	19	1		J		
Form		모,판 + C	F,R + C	자 + 편	R + F	R + F
Solution Rates	Non-Annealed @ 37.5°C (mg.cm ⁻² .hr ⁻¹)	N/A	N/A	0.0151	0.0165	0.02
Solutio	Annealed @.37.5°C (mg.cm ⁻² .hr ⁻¹)	N/A	N/A	0.0095	100.47 0.0143	0.0177
	TOTAL	99.97	100	100	100.47	5.68 1.49 0.93 0.4 1.96 2.27 100
	Sa					2.27
	Fe ₂ O ₃ NaF Ce ₂ O ₃ Se				1	1.96
	NaF				4.0	0.4
	Fe ₂ O ₃				96.0	0.93
moles	WnO				5.88 1.54 0.96 0.4	1.49
Formulation as mole%	K20 B203	6.36			5.88	5.68
Formula	K30			2		
_	MgO	19.07	20	20		
	P ₂ O ₅	46.56	_	50	47.04	45.05
	Ag10 P20s					
	CaO	27.98	30	25		17.03
	Na ₂ O CaO				26.05	25.19 17.03
Code	l	MATTOI	MATT02	MATTO3	MATT04	

R=rods; F=fibres; C=cullet

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1	4.	Proc	edure	
2				
3		4.1	Test samp	le preparation
4			4.1.1	Test samples were cut to the
5				appropriate size (see section
6				4.2.1).
7			4.1.2	Tissue culture polystyrene was
8				employed as a negative control. The
9				controls were not in the same
10				physical form as the test material.
11				
12		4.2	Fibres we	re examined in contact with the L929
13		cell	line befo	re any cleaning procedure. Fibres
14		were	examined	in contact with both cell lines
15		afte:	r cleaning	in acetone, washing in PBS and
16		ster	ilising in	a dry oven at 190°C for 2 hours.
17				
18		4.3	Cell prep	aration
19			4.3.1	A cell subculture was prepared 24
20				hours before being introduced to
21				the fibres.
22				
23		4.4	Test proc	edure
24			4.4.1	A small "bed" of the fibres was
25				placed in the bottom of each well.
26			4.4.2	The cell/medium preparation was
27				gently pipetted onto the fibre bed.
28			4.4.3	The 24-well plates were incubated
29				and examined at 24 hours and 48
30				hours.
31				

1	4.5	Interp	cetation of results
2		4.5.1	At the conclusion of the incubation period
3			the plates are removed from the incubator
4			and examined under phase contract
5			microscopy using x10 and x20 objective
6			lenses.
7		4.5.2	Each test and control material was
8			initially evaluated using the scoring
9			system detailed below. This evaluation
10			was based on the appearance of the cells
11			which were attached to the TCPS surface.
12			It was not possible to carry out such an
13			evaluation on the cells adhering to the
14			fibres.

Table 3 : Reactivity Responses

Grade	Reactivity	Conditions of all cultures
0	None	Discrete intracytoplasmic granules; no cell
		lysis
1	Slight	Not more than 20% of cells are round, loosely
		attached and without intracytoplasmic
		granules; occasional lysed cells are present
2	Mild	Not more than 50% of the cells are round and
		devoid of intracytoplasmic granules; extensive
Ì		cell lysis and empty areas between cells
3	Moderate	No more than 70% of the cell layers contain
		rounded cells and/or are lysed
4	Severe	Nearly complete destruction of the cell layers

4.6 Cytotoxicity Results

The following table highlights the results obtained following two separate tests. Two or four readings were taken at each test. In all cases negative control (TCPS) provided a 0 grade.

1 Table 4

Material Code	Grade Test 1 L9292	Material Code	Grade Test 2 L929	Test 2 HUE		
MATT01	0	MATT01	0	0		
MATT02	-	MATT02	0	0		
MATT03	-	MATT03	-	0		
MATT04	0	MATT04	0	0		
MATT05	0	MATT05	0	0		

Comments

The results as detailed provide a very subjective assessment of material cytotoxicity. Where a grade 0 is shown, there was no evidence of toxicity and a confluent healthy monolayer of cells was present. Where there was evidence of contamination or where the cell monolayer is difficult to evaluate no score has been given.

4.7 Cell Substrate Results

The following table (Table 5) details the cell-fibre interactions and general cell culture conditions observed by phase contrast microscopy. As stated before phase-contrast images of the cells on the fibres are poor. A staining procedure was carried out with the HUE cells. This procedure uses a fluorescent staining technique (ethidium bromide and acridene orange) to identify cell viability. All observations were after 48 hour contact between cells and fibres.

Table 5

										23																
MATT05	Cells are viable.	Healthy monolayer.	There is some evidence	of cell adhesion onto	the fibres.	Cells viable. Healthy	monolaver. There is	Some evidence of rell	adhesion onto the	fibres							Cells viable. Cell	بإ	healthy and equivalent	to the control wells	There is some evidence	of dell attachment but	this is difficult to	observe by phase	Contract	כסוורד מפרי
MATT04	Cells are viable.	Healthy monolayer.	There is some evidence	of cell adhesion onto	the fibres.	Cells viable. Healthy	monolayer. There is some monolayer. There is	evidence of cell	adhesion onto the	fibres.							pH is low. There Cells viable. Cell	monolayer on TCPS is	healthy and equivalent	to the control wells.	Ø	ļ.		observe by phase	contrast. (See Fig. 3) contrast	
MATT03	nation Contamination					pH is low.		be evidence of	contamination-	though this may	be degrading	glass.	Difficult to	make any comment	on cell	viability.	pH is low. There	There seems to be			though this may		glass. Difficult	to make any	comment on cell	viability.
MATT02	Contamination					Culture	medium pH	levels are	low. Cells	are viable.	There is no	obvious cell	adherence to	the fibre.			Cells are	viable. There	is no obvious evidence of		ice to	the fibre.				
MATT01	Cells are	viable.				Cells are viable Culture		granular. These	fibres are	having some	adverse effect	on the cells.					l as	sterile though granular	in appearance.	The medium pH	has dropped.	Some cells can	be seen adhering	to the fibres	(Fig. 2).	
	L929	-uou	sterile	fibres		L929	sterile	fibres									HUE	sterile	fibres							

24

- 1 The images shown in Figs. 3 and 4 were obtained
- 2 following the vital staining procedure and examined by
- 3 fluorescent microscopy.

4

- 5 In Fig. 2 the bright areas represent viable cells
- 6 (hue). The image shows an area with bundles of fibres
- 7 radiating in many directions. In most cases the cells
- 8 are rounded and not elongated on the fibres.

9

- 10 In Fig. 3 the bright areas represent viable cells
- 11 (hue). Cells can be seen elongated on the fibres. In
- 12 this image most of the fibres are oriented in the same
- 13 direction. There is excellent cell coverage. This
- 14 image is also representative of the result obtained
- 15 with MATTO5.

16

- 17 Of the five fibre compositions examined, MATT04 and
- 18 MATT05 are providing an excellent substrate for cell
- 19 adhesion. MATT01 has large numbers of cells adhering
- 20 although the cell morphology is more rounded than that
- 21 seen on the control surface. MATT02 and MATT03 show
- 22 cells adhering but in much reduced numbers. There is
- 23 no evidence of cytotoxicity with any of the fibres
- 24 examined.

- 26 As well as demonstrating cell viability the procedure
- 27 permitted a better evaluation of the cells attaching to
- 28 the fibres. The cell-fibre interaction was much better
- 29 than that indicated by phase contrast microscopy. It
- 30 was noted that MATT04 and MATT05 had excellent cell
- 31 adherence. MATT01 permitted a good cell adherence.
- 32 There was cell attachment with MATT02 and MATT03

32

1	although this was poor in comparison with 01, 04 and
2	05.
3	•
4	Example 3
5	
6	A cell suspension (in complete cell culture medium
7	supplemented with 5% foetal calf serum) at a
8	concentration of approx. 5×10^5 cell/ml was introduced
9	to an established mouse fibroblast cell line (L929).
10	
11	The material/cell interaction was examined using phase
12	contrast microscopy at 24, 48 and 72 hours. In
13	particular the following materials were examined (see
14	Table 6 for composition of the glasses referred to by
15	batch number).
16	
17	a) Glass sheet (flat); code 1051098-1
18	
19	Cells can be seen adhering to the material and remain
20	in contact with the material following sequential
21	transfer between dishes. The cell morphology is
22	rounded and the growth rate is considerably slower than
23	observed with cells on the control dishes.
24	Nevertheless there is evidence of cell division taking
25	place on the surface.
26	
27	b) Sintered glass beads (smooth surface); code BX-
28	D221098-1, Sintered glass beads (rough surface);
29	code BX-D221098-1
30	
31	It is more difficult to make the observations with

these samples using phase contrast. However, cells are

26

- 1 clearly present on the surface of both rough and smooth
- 2 samples. The cell population is certainly increasing
- 3 with time up to the 72 hour period. Again, this is
- 4 following sequential transfer at 24 hours.

Table 6

Batch Number	1	ulation mole%		Total	Soluti	Physical Form		
	Na ₂ O CaO F		P ₂ O ₅		Annealed @37.5°c (mg.cm'2 .hr'1	Annealed @37.5°c (mg.cm'2. hr'1		
1051098 -1	25	28	47	100	0.0991	0.1364	R+S	
D221098 -1	11	42	47	100	0.0377	0.0446	G+R	

G=GRANULES R=RODS S=SHEETS

- 5 Sample SEMs were obtained (see Figs. 4 to 7) after
- 6 cells had been in contact with the glass for 72 hours,
- 7 fixed in 2.5% glutaraldehyde and dehydrated with
- 8 alcohol. The samples were gold coated before viewing.
- 9 The magnification is indicated on Figs. 4 to 7.

10 11

Example 4

- 13 The potential for using CRG glass releasing two
- 14 different kinds of metallic ions or boron as a cell
- 15 culture growth substrate has been assessed for L929
- 16 mouse fibroblast cell line. To do so extraction
- 17 vehicles were prepared which combined extracts of a
- 18 mixture of two CRG's releasing a different type of
- 19 metallic ions or boron, then it was determined at which
- 20 concentration a positive effect on the metabolic

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activity of an L929 mouse fibroblast cell line was obtained. This data would give a good indication of the potential of these combined CRG as matrix for cell growth substrates according to the invention. Materials The materials used in this investigation were control release glasses (CRG's) containing silver (Ag), copper (Cu), magnesium (Mg), zinc (Zn), nickel (Ni) ions and boron (B). The glasses were pre-ground to a particle size < 53 $\mu\text{m}\,.$ The composition of the CRG's are shown in Table 7 below, along with information on dissolution rates. The extraction vehicles used were PBS (phosphate buffered solution - similar to fluids found in the body) and MEM (199 Modified Earles Medium -containing serum proteins).

28

1 Table 7

2

3 CRG Composition and Dissolution Rates

4

CRG	Na ₂ O	CaO	P ₂ O ₅	Ion	Dissolution	Dissolution
	(mol%)	(mol%)	(mo1%)	(mol%)	Rate	Rate
					(Mg/cm²/hr)	(Mg/cm²/hr)
					(annealed)	(non-
			<u>.</u>			annealed)
Ag	32	18	47	3	0.5673	0.9413
Cu	31	15	47	7	0.6608	0.9973
Mg	38	9	47	6	0.9764	1.4004
Zn	31	14	47	8	1.5638	0.9232
Ni	32	18	47	3	0.2166	0.2999
В	41.5	_	41.5	17	0.1188	0.1744

5 6

Establishing an L929 mouse fibroblast cell line

7 8

- The cell line was established by subculturing an
- 9 already existing cell line that was maintained by the
- 10 University of Liverpool. The cells are maintained in
- 11 199 Modified Earles Medium (MEM), and stored in
- 12 incubation at 37° C in a 5% $CO_2/95\%$ air atmosphere. The
- 13 cells were grown to confluence in a flat-bottomed
- 14 flask, and the monolayer was then harvested using
- 15 trypsinization. The subculturing was carried out under
- 16 sterile conditions using a laminar flow hood, and the
- 17 following protocol was followed:

18 19

Fibroblast Subculturing Protocol

- Take the original flask containing 10 ml of MEM, and
 check the cells under the microscope.
- 3 Place the flask under the laminar flow hood and
- 4 remove the MEM using a sterile glass pasteur and
- 5 vacuum.
- Add 2.5 ml of 1% trypsin to the flask to loosen the
- 7 confluent layer of cells. Observe the loosening of
- 8 the cells under the microscope (it takes approx 3-4
- 9 mins).
- 10 Once the cells are loosening (they take on a rounded
- 11 appearance) return the flask to the hood and remove
- the trypsin using a pasteur and the vacuum, replace
- with 10 ml of fresh MEM.
- The flask is then agitated gently to remove the cells
- from the base, forming a suspension of approximately
- 16 10⁶ cells/ml concentration.
- 1 ml of this suspension is then added to 9 ml of
- 18 fresh MEM in a fresh flask. Two flasks are prepared
- in this manner.
- 20 Finally the flasks are labelled with name, date and
- cell line. The cells are then returned to the
- incubator and left for a week to establish a
- 23 confluent layer of cells.

- 25 Subculturing then takes place once a week, with two
- 26 subculturing flasks being prepared at a 1 in 10
- 27 concentration (then left for a week to develop a
- 28 confluent layer), and the 96 well microtitre plates
- 29 being prepared at a 1 in 40 concentration. The
- 30 estimated cell concentration when the layer is
- 31 confluent is 1×10^6 cells/ml.

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30

1 Preparing the Extraction Vehicles

2

- 3 0.1 g of each of the CRG's making up the combinations
- 4 was weighed out using a microbalance. The CRG's were
- 5 placed into a sterile universal container and to this
- 6 20 ml of the extraction vehicle was added i.e. PBS or
- 7 MEM. The extraction vehicles were then incubated at
- 8 37° C in a 5% $CO_2/95\%$ air atmosphere for a period of four
- 9 hours. Four hours was selected as the CRG's had
- 10 completely dissolved in the PBS within this time, and
- 11 began to precipitate out if left for longer. The CRG's
- 12 had still not dissolved fully when left in MEM for a
- 13 period of 72 hours, and so it was decided to use four
- 14 hours for both extraction vehicles. After this time
- 15 they were removed from the incubator and filtered under
- 16 sterile conditions. The filtering was performed to
- 17 remove any contamination and precipitates.

18

- 19 The next step was to prepare the range of
- 20 concentrations. The filtered extract (20 ml) was
- 21 initially added to 20 ml of double strength culture
- 22 medium to provide a starting concentration of 50% in a
- 23 single strength medium. This concentration was not
- 24 used during the tests. Next, 10 ml of MEM was measured
- 25 out into a fresh universal container and 10 ml of 50%
- 26 solution added to provide a 25% concentration, this was
- 27 further diluted in MEM until a concentration of 0.05%
- 28 had been established.

- 30 1. 10 ml 50.0% solution + 10 ml fresh MEM = 25.0%
- 31 concentration*.

1 :	2.	10	ml	25.0%	solution	+	10	ml	fresh	MEM	=	12.5	5 응
-----	----	----	----	-------	----------	---	----	----	-------	-----	---	------	-----

- 2 concentration*.
- 3 3. 10 ml 12.5% solution + 10 ml fresh MEM \approx 6.25%
- 4 concentration*.
- 5 4. 10 ml 6.25% solution + 10 ml fresh MEM = 3.12%
- 6 concentration.
- 7 5. 10 ml 3.12% solution + 10 ml fresh MEM = 1.60%
- 8 concentration*.
- 9 6. 10 ml 1.60% solution + 10 ml fresh MEM = 0.80%
- 10 concentration.
- 11 7. 10 ml 0.80% solution + 10 ml fresh MEM = 0.40%
- 12 concentration*.
- 13 8. 10 ml 0.40% solution + 10 ml fresh MEM = 0.20%
- 14 concentration.
- 15 9. 10 ml 0.20% solution + 10 ml fresh MEM = 0.10%
- 16 concentration*.
- 17 10. 10 ml 0.10% solution + 10 ml fresh MEM = 0.05%
- 18 concentration*.

19

20 * Concentrations used throughout the test.

21

22 Setting up the well plates

23

- 24 The well plates were seeded with a 1 in 40
- 25 concentration of fibroblasts. The medium was pipetted
- 26 into the wells using a pipetter and a sterile trough.
- 27 A 1 in 40 concentration was chosen as the effects on
- 28 the growth of the cells was being investigated and so a
- 29 confluent layer was not required.

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32

1 The plates were then re-incubated at 37°C in a

- 2 5%/CO₂/95% air atmosphere) for a period of 48 hours or
- 3 96 hours. After this time, the medium was removed from
- 4 the plates under sterile conditions and replaced with
- 5 the prepared exudates in the following manner. Twelve
- 6 wells were used for each concentration, and again the
- 7 pipetter and sterile troughs were used to deliver the
- 8 extraction of vehicles to the wells.

9

Control	12.5%	1.6%	0.1%
12 wells	12 wells	12 wells	12 wells
25%	6.25%	0.4%	0.05%
12 wells	12 wells	12 wells	12 wells

10

11 The plates were then incubated (at 37° C in a 5% $CO_2/95$ %

- 12 air atmosphere) for a further period of 48 hours or 72
- 13 hours, after which the extraction vehicle was removed
- 14 and an MTT assay was performed.

15

Performing the MTT Assay

- 18 The MTT assay is a rapid colomeric assay based on the
- 19 tetrazolium salt MTT (3- (4,5-dimethylthiazol-2-yl)-
- 20 2,5-diphenyl tetrazolium bromide). The cells produce
- 21 certain enzymes when they are growing, and the MTT salt
- 22 solution is cleaved into blue formazan crystals by one
- 23 such enzyme reportedly the "mitochondrial enzyme
- 24 succinate-dehydrogenase". The crystals are soluble in
- 25 iso-propranol and produce a coloured aqueous solution.
- 26 The amount of formazan produced is said to be
- 27 proportional to the number of viable cells present i.e.

- the darker the shade of blue produced indicates a
- 2 greater level of cell activity.

- 4 200 μ l of MTT salt solution was added to each well in
- 5 the plates at a concentration of 1 mg/ml and the plates
- 6 were then incubated at 37° C for a period of four hours.
- 7 The MTT solution was then removed and replaced with
- 8 approximately 100 μ l of iso-propranol. The plates were
- 9 then incubated for a further 20 minutes (at 37°C). To
- 10 ensure complete dissolution of the blue formazan
- 11 crystals the plates were gently shaken.

12

- 13 The final stage was to measure the optical density
- 14 readings of the plates using an enzyme-linked
- 15 immunosorbent assay (ELISA) plate reader at a test
- 16 wavelength of 570 nm.

17

- 18 The repetition for the results was obtained by using 12
- 19 wells in the 96 well plate for each of the
- 20 concentrations and the control. Repetition was
- 21 required to reduce the amount of error involved with
- 22 the results.

23

- 24 So that the results were comparable, various different
- 25 steps were taken. These included:

- The dissolution time for each extraction vehicle for
- 28 four hours.
- The incubation times were the same for each exudate,
- 30 either two days in MEM followed by two days with the

exudate (2d-2d), or four days in MEM followed by 1 three days with the exudate (4d-3d). 2 • The cells were kept at constant conditions throughout 3 the investigation, $37^{\circ}C/5\%$ CO_2 . 4 5 The results obtained have been displayed as bar charts 6 and are shown in Figs. 8 to 20. The important features 7 to consider on the charts are the set numbers and the 8 cell activity levels. Each of the set number 9 correlates to a different concentration as follows: 10 11 Control Set One : 12 Set Two 25% 13 : 12.5% 14 Set Three : 6.25% Set Four : 15 1.6% Set Five 16 : 0.4% 17 Set Six : Set Seven 0.1% 18 : 0.05% Set Eight : 19 20 The control used throughout the study was cells at a 1 21 in 40 concentration proliferating in 5% MEM with added 22 fetal calf serum and antibiotics. This control was 23 used because it gave a good indication of the accuracy 24 of the MTT assay, and could be easily used to determine 25 whether the combinations were antagonising or 26 27 synergising cell growth.

28

29 To obtain the cell activity level from the optical

30 density readings the control was fixed to the level of

one, the remainder of the optical density readings

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- 1 obtained were then adjusted in accordance with this
- 2 level. This means that by observing the charts it is
- 3 easy to determine whether the combinations are having a
- 4 positive or negative effect on the cell growth.

- 6 Several of the optical density readings could not be
- 7 counted by the ELISA plate when the cells were left for
- 8 the longer period of time. The amount of cell activity
- 9 was greater than the range of the plate reader.
- 10 However, these results are known to be at least three,
- 11 and so have been added to the results as this minimum
- 12 value. Results where this has occurred are marked with
- 13 an * on the charts.

14

15 Results

16

17 Ag/Mg in a PBS Extraction Vehicle (Fig. 8)

18

- 19 The graph of Fig. 8 shows a stimulation response
- 20 evident for the 2d-d2 sample over the range 6.25% to
- 21 0.05%, with the peak stimulation occurring at a
- 22 concentration of 0.05%, exhibiting a 28% increase on
- 23 the control level.

24

25 Ag/Ni in a PBS Extraction Vehicle (Fig. 9)

- 27 The graph shown in Fig. 11 shows a stimulatory effect
- 28 occurring during the 2d-2d period. There is a
- 29 stimulation taking place at 0.05%, and being 15% above
- 30 the control. No result was obtained for 12.5% for 2d-
- 31 2d as it was not initially selected in the range of
- 32 concentrations.

Aq/Zn in an MEM Extraction Vehicle (Fiq. 10) 1 2 There is evidence of this combination reacting 3 toxically to the cells at high concentrations (25%, 4 12.5% and 6.25%) for both length of times. However, 5 for the lowest concentrations of 0.1% and 0.05% cell 6 proliferation has been induced. The stimulation for 7 the shorter time period is greater than for 4d-3d, with 8 a 17% increase on the control level at 0.05%. 9 10 Ag/B in a PBS Extraction Vehicle (Fig. 11) 11 12 The analysis of the graph represented in Fig. 11 shows 13 that for 2d-2d periods the stimulation of the cell 14 metabolism begins at 12.5%, with the peak occurring at 15 0.05%, 40% above the control. For the 4d-3d period, a 16 stimulatory effect of 5% above the control occurs at 17 the 0.05% concentration. 18 19 Mg/Cu in a PBS Extraction Vehicle (Fig. 12a) 20 21 The graph of Fig. 12a shows that a stimulatory response 22 occurs for the 2d-2d time period for concentrations 23 between 6.25% and 0.4% with a peak being displayed at 24 6.25%, indicating a 28% increase on the control. 25 26 Considering the ions individually, magnesium is known 27 to be fairly non-toxic ion even in the high 28 concentrations, however, copper ions are extremely 29 toxic at high concentrations. This would suggest that 30

by combining the copper with the magnesium, the

magnesium is suppressing the affect of the copper over 1 this particular range for the PBS. 2 3 Mq/Cu in an MEM Extraction Vehicle (Fig. 12b) 4 5 The graph of Fig. 12b shows that cell proliferation 6 occurs at the lower concentrations, (0.4%, 0.1% and 7 0.05%) for the 4d-3d samples. A peak occurs at 0.05% 8 indicating a 33% increase on the control levels of 9 cells. The 4d-3d time period also exhibits a gradual 10 increase from toxicity to stimulation. 11 12 Mg/Ni in a PBS Extraction Vehicle (Fig. 13) 13 14 The 2d-2d time period exhibits very interesting 15 behaviour with a stimulatory peak occurring at a 16 concentration of 1.6%, indicating a 24% increase on 17 cell metabolism above the control. A stimulatory 18 response also occurs at 6.25% and 0.05%. 19 20 Mg/B in a PBS Extraction Vehicles (Fig. 14a) 21 22 This CRG combination produces a significant stimulatory 23 effect for the 2d-2d period, with stimulation being 24 apparent from 0.05% up to 1.6% (although 0.1% is just 25 below the control). The peak in this positive effect 26

29

control level.

27

28

30 Mg/B in an MEM Extraction Vehicle (Fig. 14b)

occurs at a concentration of 1.6% and is 32% above the

- 1 The graph of Fig. 14b shows that there is a very small
- 2 toxic effect on the metabolism of the cells in both of
- 3 the chosen time periods. In fact the cell activity
- 4 levels for concentrations between 25% and 1.6% are
- 5 fairly equal. For the 4d-3d time, a stimulatory effect
- 6 is present from 0.4% onwards. The maximum stimulation
- 7 occurs at 0.05% and is 14% above the control.

8

9 <u>Ni/Cu in a PBS Extraction Vehicle (Fig. 15a)</u>

10

- 11 The graph of Fig. 15a shows high levels of toxicity
- 12 occurring at the high concentrations 25% and 12.5% for
- 13 both lengths of time. For the 2d-2d time there is a
- 14 sudden increase in the cell activity to just 7% below
- 15 the control at the 6.25% CRG concentration. Cell
- 16 metabolism stimulation can be seen from 1.6% onwards
- for 2d-2d, and 0.4% for the 4d-3d. Both time periods
- peak at 0.05%, at approximately the same level 12/13%.
- 19 Ni/Cu in an MEM Extraction Vehicle (Fig. 15b)

20

- 21 A toxic effect can be seen at the high concentrations
- 22 for both time periods as with many of the other
- 23 combinations. The toxicity levels are then
- 24 significantly lower at 1.6%. For the 4d-3d time there
- is evidence of stimulation from 0.4% through to 0.05%,
- 26 with both 0.1% and 0.05% stimulating by 15% above the
- 27 control. There is a sign of stimulation in the 2d-2d
- 28 time at 0.1%, however, it is only 1.5% above the level
- 29 of the control.

30

31 Ni/Zn in an MEM Extraction Vehicle (Fig. 16)

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39

- 1 The main feature of the graph of Fig. 16 is the
- 2 stimulation peak for the 2d-2d time at a concentration
- of 0.1%, 12% above the control. The stimulation peak
- 4 for 4d-3d at the 0.05% concentration approximately 8%
- 5 above the control, and toxic effects are present at the
- 6 high concentrations. There is a sharp increase in the
- 7 cell activity between 6.25% and 1.6%.

8

9 Ni/B in a PBS Extraction Vehicle (Fig. 17a)

10

- 11 This combination elicits a stimulatory response on the
- 12 cell metabolism over the concentration range 1.6% to
- 13 0.05% for the 2d-2d with a maximum occurring at a
- 14 concentration of 0.1%, 25% above the control. There is
- 15 a gradual increase in the activity of the cells over
- 16 the 4d-3d period, with non-toxicity being reached at
- 17 0.1%, and a peak occurring at 0.05%, 17% above the
- 18 control.

19

20 Ni/B in an MEM Extraction Vehicle (Fig. 17b)

21

- 22 The results shown in the graph of Fig. 17b for the 2d-
- 23 2d period are high toxicity at the high concentrations
- 24 with a gradual increase in the cell activity over the
- 25 range. There is a positive effect occurring due to
- 26 this combination. There is stimulation from 12.5%
- onwards, peaking at 0.05%, 33% above the control.

28

29 <u>Cu/Zn in an MEM Extraction Vehicle (Fig. 18)</u>

- 31 The graph in Fig. 18 shows that this combination
- 32 elicits a toxic response at the higher concentrations

- 1 (25% through to 6.25%). The cell growth ceases to be 2 affected at 0.05% for the 2d-2d time. There is cell
- 3 proliferation occurring in the 4d-3d set of results
- 4 from 0.4% onwards. The maximum stimulation occurs at
- 5 0.05%, with a significant increase of 42% on the
- 6 control level.

7

8 Cu/B in an MEM Extraction Vehicle (Fig. 19)

9

- 10 Considering the graph of Fig. 19, it is noticeable that
- 11 there is a gradual increase in the cell activity for
- 12 both 2d-2d and 4d-3d. At 25% the combination elicits a
- 13 toxic effect on the cells and at 0.05% it produces cell
- 14 proliferation. It is 20% above the control for 2d-2d,
- and 28% above the control for the 4d-3d.

16

17 Zn/B in a PBS Extraction Vehicle (Fig. 20)

18

- 19 Considering the graph of Fig. 20 there is evidence of
- 20 toxicity at the high concentrations (25%, 12.5% and
- 21 6.25%) for both time periods. The stimulatory effect
- 22 by the cells to this combination for the 2d-2d period
- 23 begins at a concentration of 1.6% and peaks at 0.1%,
- 24 27% greater than the control level.

2526

Conclusion

- 28 The results collected show that CRG releasing various
- 29 combinations of metallic ions and boron have potential
- 30 as a matrix in a cell culture growth substrate
- 31 according to the invention. This is the case in
- 32 particular for combinations containing boron where in

- 1 some combinations the stimulation is 25% greater than
- 2 the control.

1	CLAI	MS
2		
3	1.	A cell culture growth substrate comprising a water
4		soluble glass matrix adapted to sustain growth of
5		living cells.
6		
7	2.	The substrate of Claim 1, wherein at least a
8		portion of the surface of said substrate is coated
9		with living cells.
10		
11	3.	The substrate of Claim 1 or 2, wherein said matrix
12		has at least a portion of its surface coated with
13		living cells.
14		
15	4.	The substrate of any one of Claims 1 to 3, wherein
16		the water-soluble glass is a phosphate glass.
17		
18	5.	The substrate of any one of Claims 1 to 4, wherein
19		said water-soluble glass comprises phosphorous
20		pentoxide as glass former.
21		
22	6.	The substrate of any one of Claims 1 to 5, wherein
23		said glass comprises an oxide or a carbonate of an
24		alkali metal, an alkaline earth metal or a
25		transition metal as glass modifier.
26		
27	7.	The substrate of Claim 6, wherein said glass
28		modifier is sodium oxide, potassium oxide,
29		magnesium oxide, zinc oxide or calcium oxide.

		13
1	8.	The substrate of any one of Claims 1 to 7, wherein
2		said water-soluble glass contains a boron
3		containing compound.
4		
5	9.	The substrate of any one of Claims 1 to 8, wherein
6		said glass has a dissolution rate ranging from
7		substantially zero to 2.0 mg/cm²/hour at 38°C.
8		
9	10.	The substrate of any one of Claims 1 to 9, wherein
10		said glass enables a controlled release of
11		additives in an aqueous medium.
12		
13	11.	The substrate of Claim 10, wherein said additives
14		comprise at least one metallic ion or boron.
15		
16	12.	The substrate of any one of Claims 1 to 11,
17		wherein said water-soluble glass matrix comprises
18		water-soluble glass fibres.
19		
20	13.	The substrate of Claim 12, wherein said glass
21		fibres are sintered together to form non-woven
22		mat.
23		
24	14.	The substrate of any one of Claims 1 to 10,
25		wherein said water-soluble glass matrix comprises
26		finely comminuted glass particles.
27		
28	15.	The substrate of Claim 14, wherein said finely
29		comminuted glass particles are sintered together
30		to form a porous structure.

44

The substrate of Claim 14 or 15, wherein said 1 16. glass particles have an average diameter of from 2 15 microns to 6 mm. 3 4 17. Use of the substrate of any one of Claims 1 to 16 5 as an implant to replace or promote repair of 6 damaged tissue in a patient. 7 8 A method to encourage growth of living tissue by 9 18. 10 providing the substrate of Claims 1 to 16. 11 Method of Claim 18, wherein said method includes 12 19. the step of delivering metal ions or boron to an 13 aqueous medium at a rate which maintains a 14 concentration of metal ions or boron in said 15 aqueous medium of not less than 0.01 parts per 16 million and not greater than 10 parts per million. 17

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(54) Title: CELL GROWTH SUBSTRATE

(57) Abstract: A cell culture growth substrate comprising a water soluble glass matrix adapted to sustain growth of living cells. Preferably the substrate comprises or is coated with living cells. The water-soluble glass is advantageously phosphate based and comprises glass fibres or finely comminuted particles. The invention also relates to the use of the growth substrate as an implant to replace or promote repair of damaged tissue in a patient and to a method to encourage growth of living tissue.

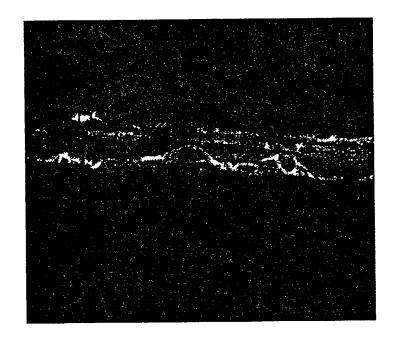


Fig. 1

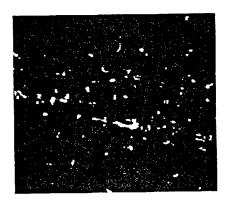


Fig. 2

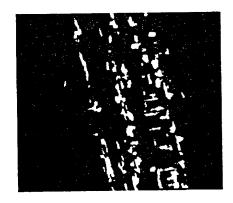


Fig. 3

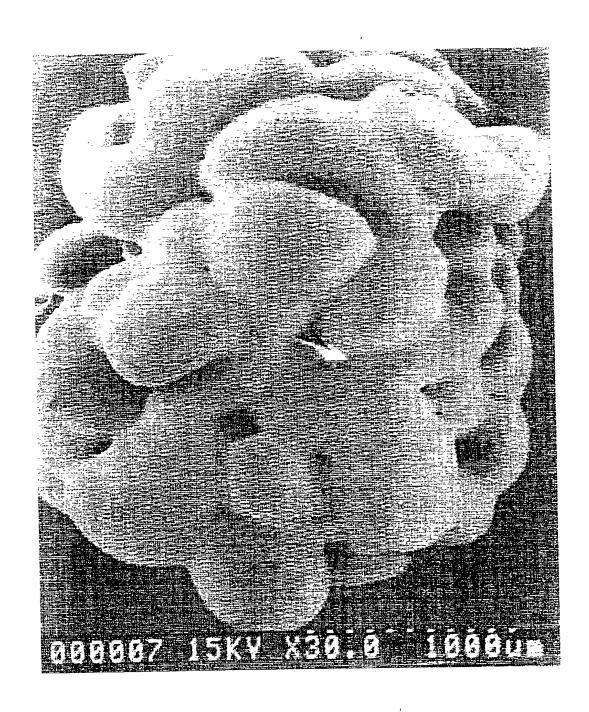


Fig. 4

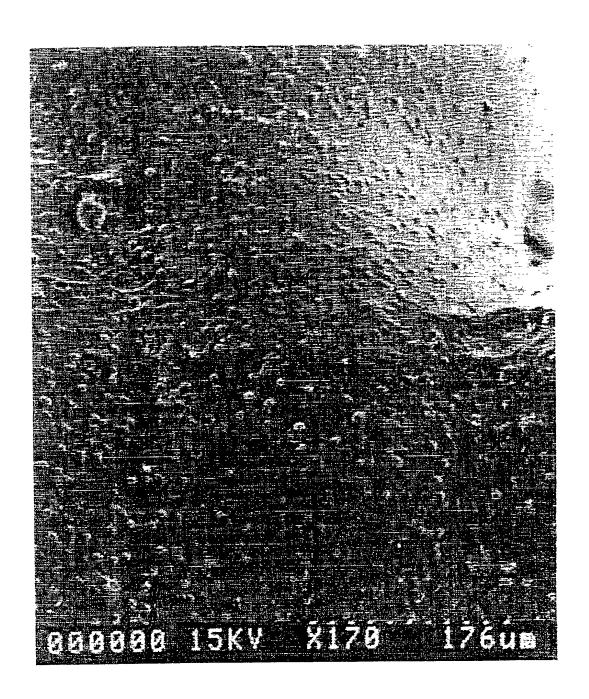


Fig. 5

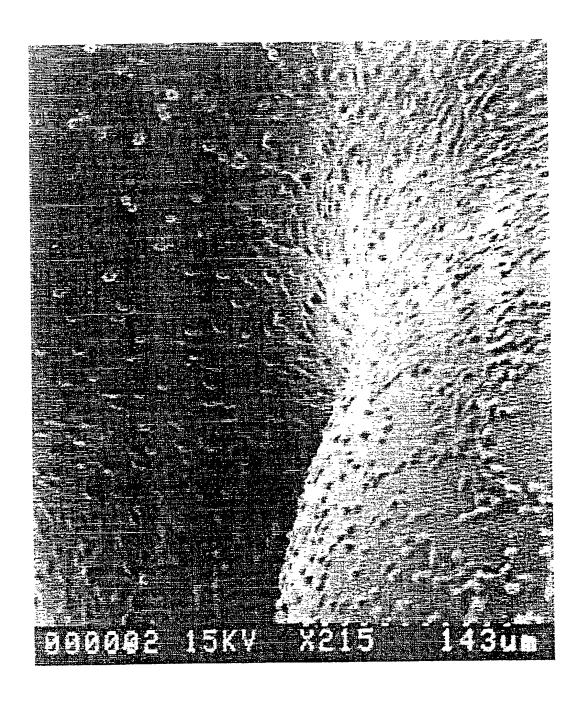


Fig. 6

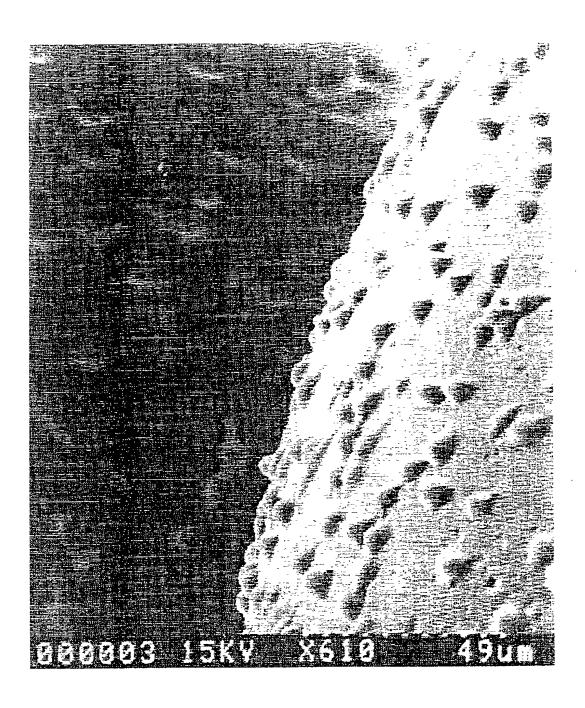
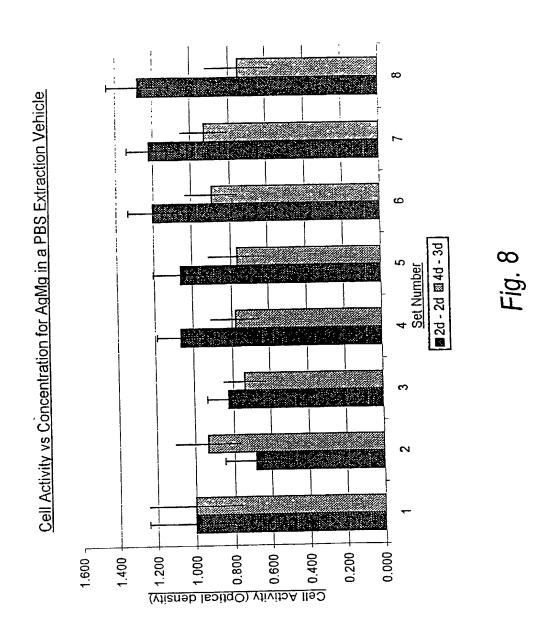
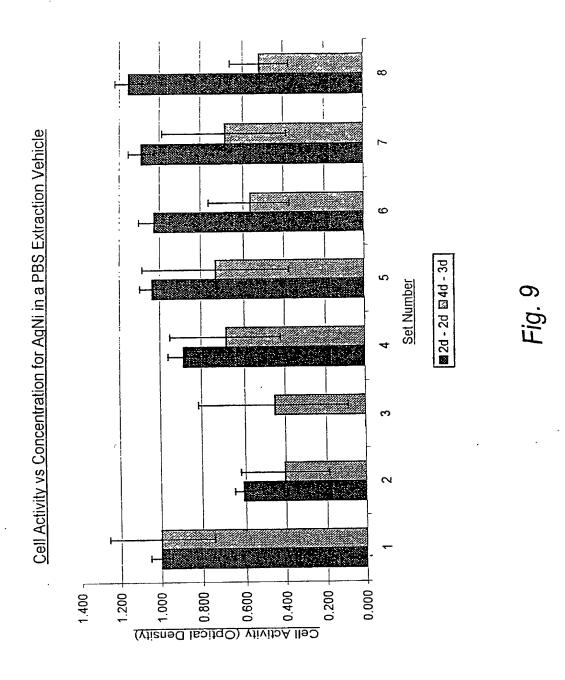


Fig. 7

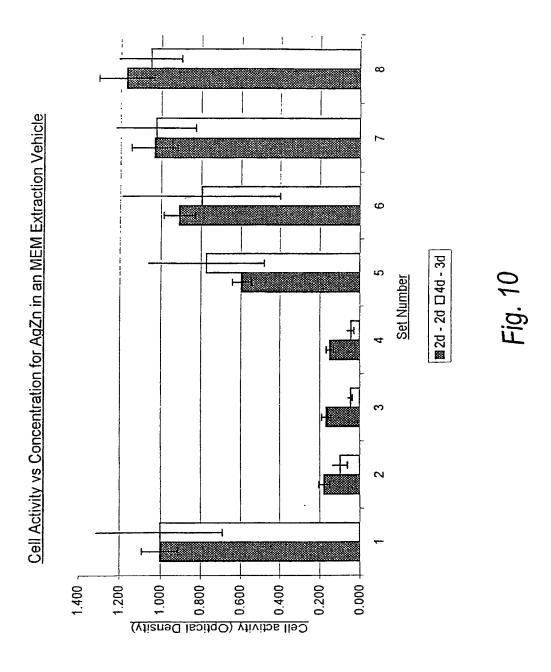
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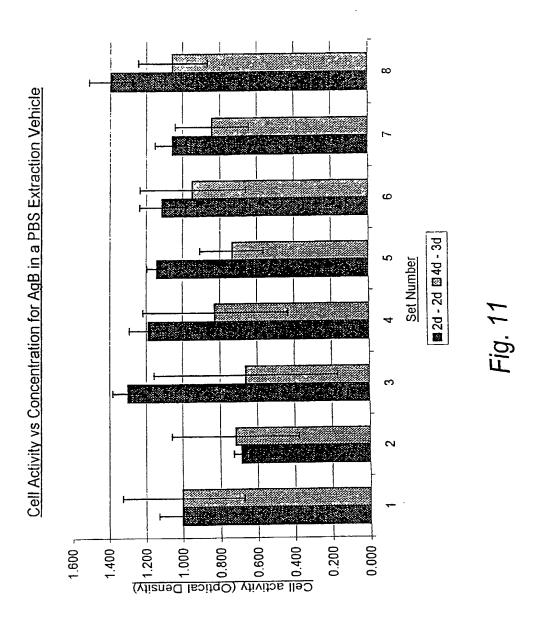


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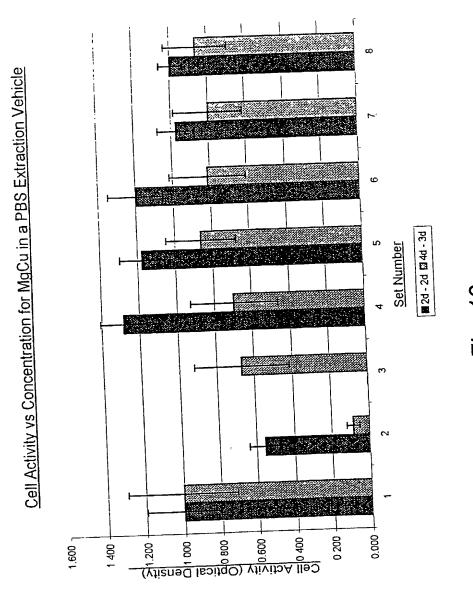
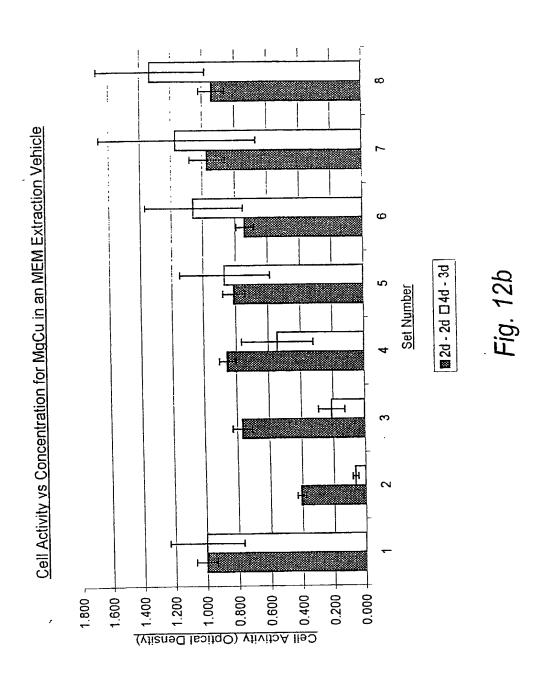
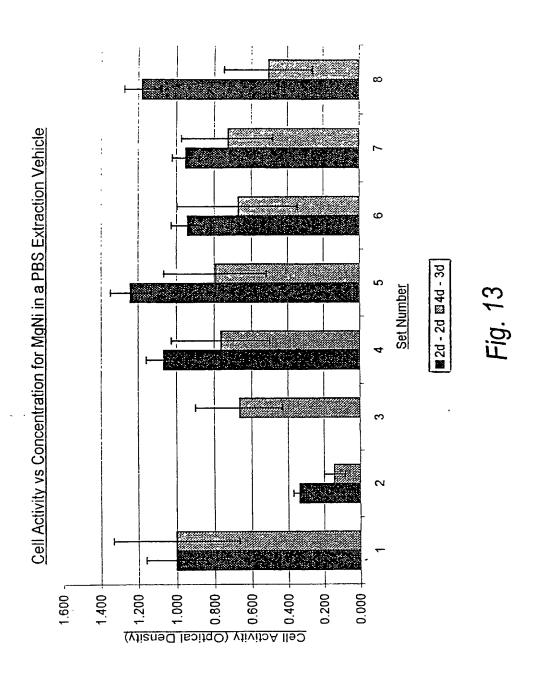


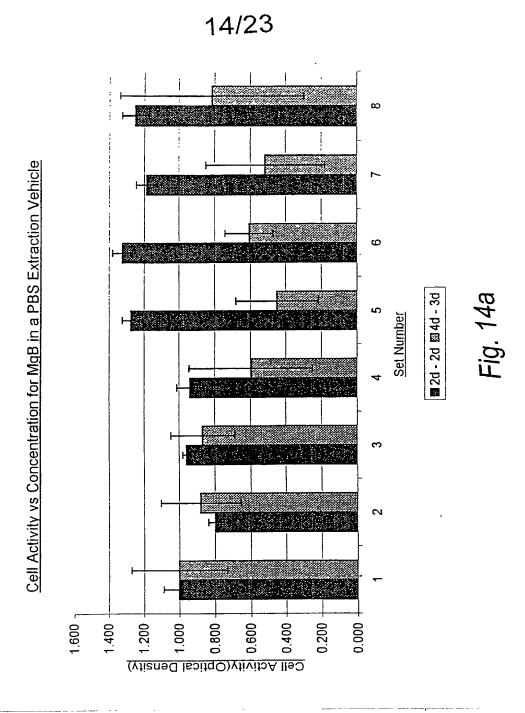
Fig. 1'2a

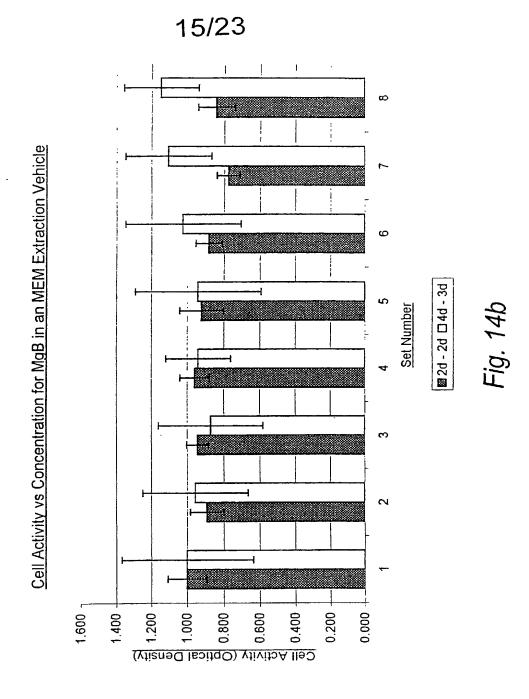




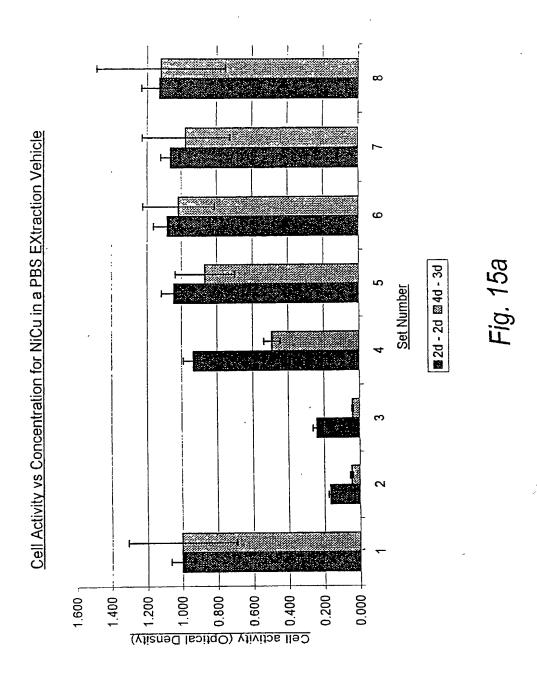
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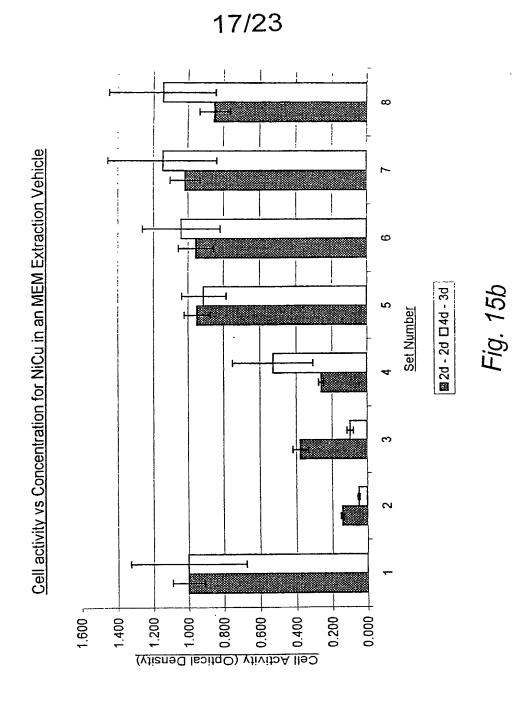




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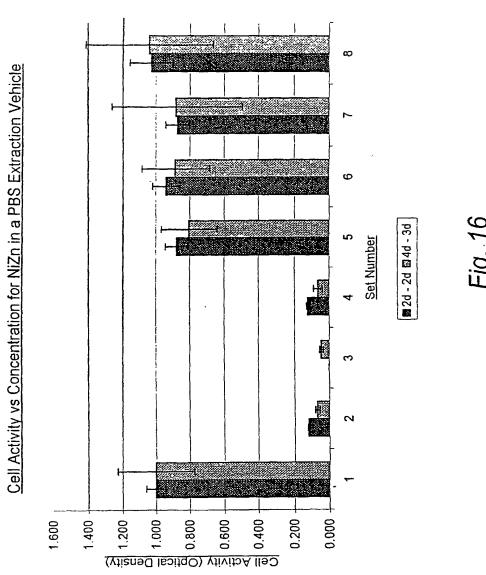


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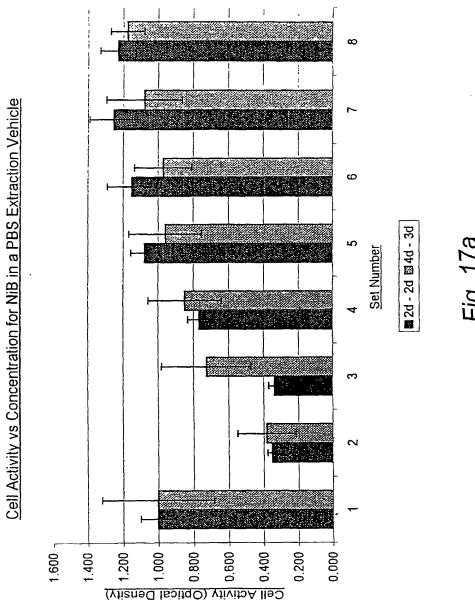


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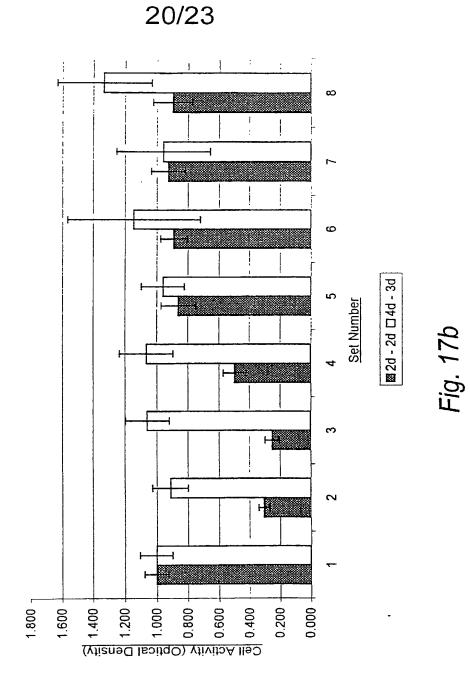


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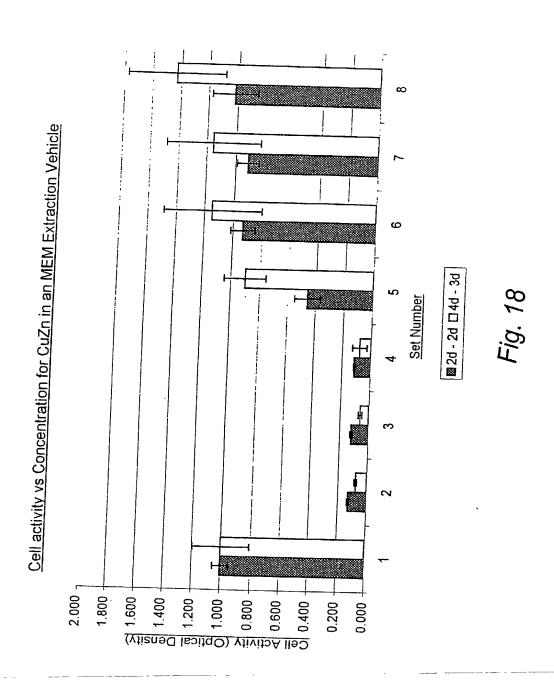


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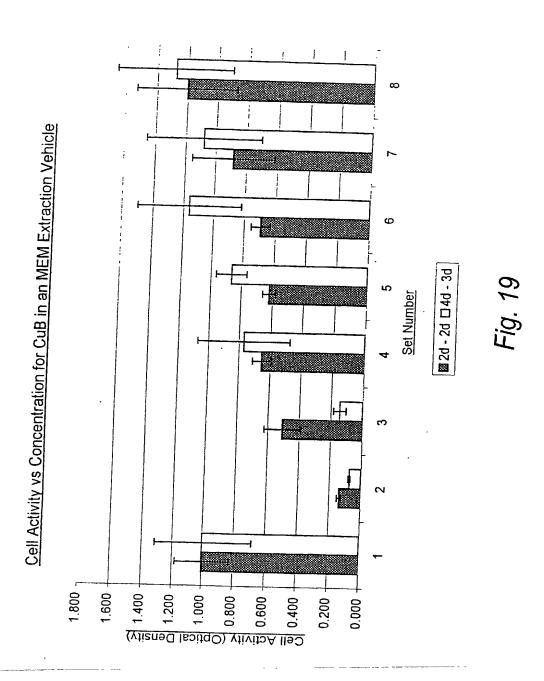


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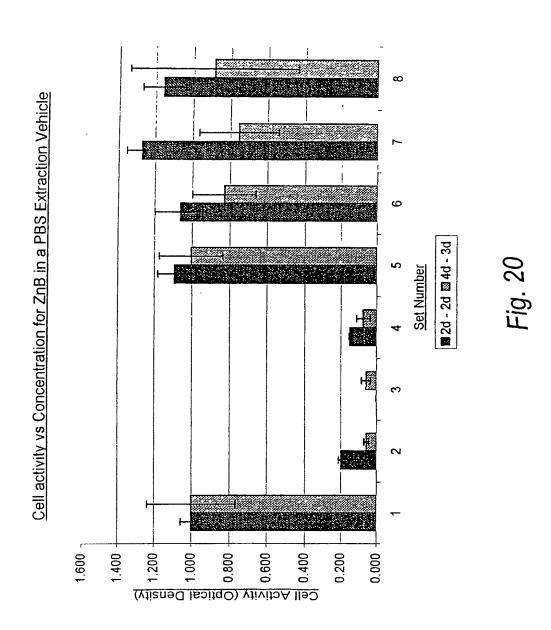


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United States Patent Application

COMBINED DECLARATION AND POWER OF ATTORNEY

Attorney's Docket Number	
As a below named inventor, I hereby declare that:	
My residence, post office address and citizenship are as stated below next to my name.	

I believe I am the original, first and sole inventor (if only one name is listed below) or an original, first and joint inventor (if plural names are listed below) of the subject matter which is claimed and for which a patent is sought on the invention entitled:

"Cell Growth Substrate"

the specification of which:

[c] was filed as a PCT International Application Number PCT/GB00/03424 on 7 September 2000.

I hereby state that I have reviewed and understand the contents of the above-identified specification, including the claims, as amended by any amendment referred to above.

I acknowledge the duty to disclose information which is material to the examination of this application in accordance with 37 CFR §1.56.

I hereby claim foreign priority documents under 35 U.S.C §119(a)-(d) or §365(b) of any foreign application(s) for patent or inventor's certificate, or §365(a) of any PCT international application which designated at least one country other than the United States, listed below and have also identified below any foreign application for patent or inventor's certificate or PCT international application having a filing date before that of the application on which priority is claimed:

PRIOR FOREIGN/PCT APPLICATION(S)

COUNTRY	APPLICATION NUMBER	DATE OF FILING	PRIORITY CLAIMED
United Kingdom	9920974.4	07.09.1999	YES
United Kingdom	9927802.0	25.11.1999	YES

I hereby claim the benefit under 35 U.S.C §120 of any United States application(s) or §365(c) of any PCT international application(s) designating the United States, listed below and, insofar as the subject matter of each of the claims of this application is not disclosed in the prior United States application in the manner provided by the first paragraph of 35 U.S.C. §112, I acknowledge the duty to disclose material information as defined in 37 CFR §1.56 which become available between the filing date of the prior application and the national or PCT international filing date of this application:

PRIOR US APPLICATIONS OR PCT INTERNATIONAL APPLICATIONS DESIGNATING THE US FOR BENEFIT UNDER 25 U.S.C §120

APPLICATION No. DATE OF FILING PATENTED PENDING ABANDONED

POWER OF ATTORNEY: As a named inventor, I hereby appoint the following attorney(s) and/or I I I agent(s) to prosecute this application and transact all business in the Patent and Trademark Office connected therewith:

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I acknowledge the duty to disclose information which is material to the examination of this Application in accordance with Title 37, Code of Federal Regulations, Section 1.56(a).

I hereby declare that all statements made herein of my own knowledge are true and that all statements made on the information and belief are believed to be true; and further that these statements were made with the knowledge that wilful false statements and the like so made are punishable by fine or imprisonment, or both, under Section 1001 of Title 18 of the United States Code, and that such wilful false statements may jeopardize the validity of the Application or any Patent issuing thereon.

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